

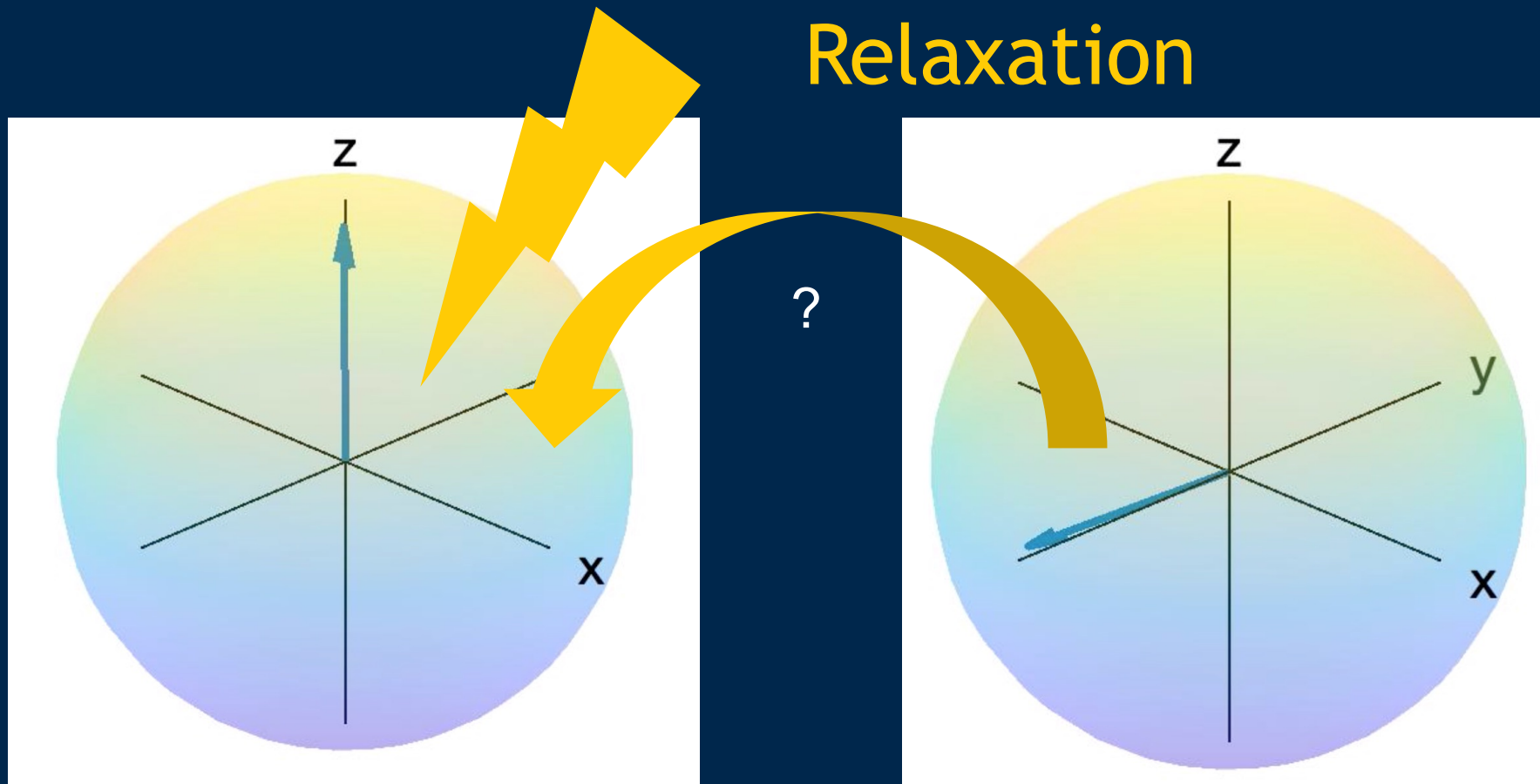
# MRI Physics:

# T1 Relaxation

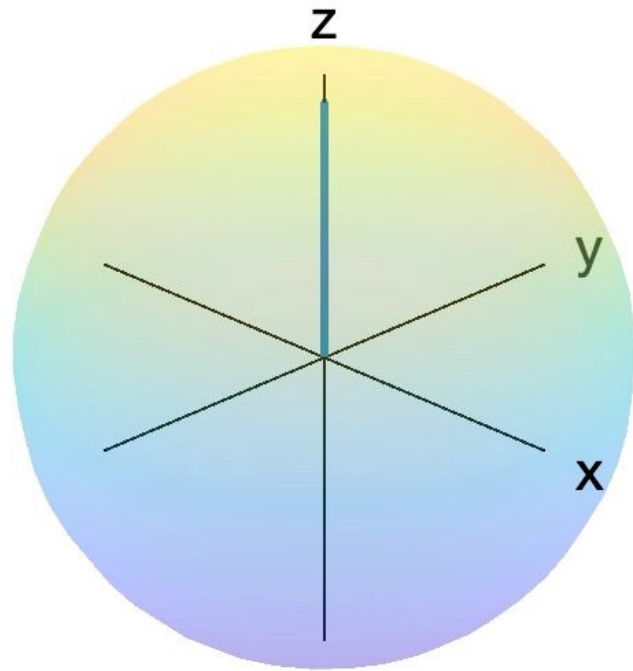
Nicole Seiberlich  
Associate Professor, Radiology  
Co-Director of MIITT

# We tip magnetization into x-y plane for signal acquisition

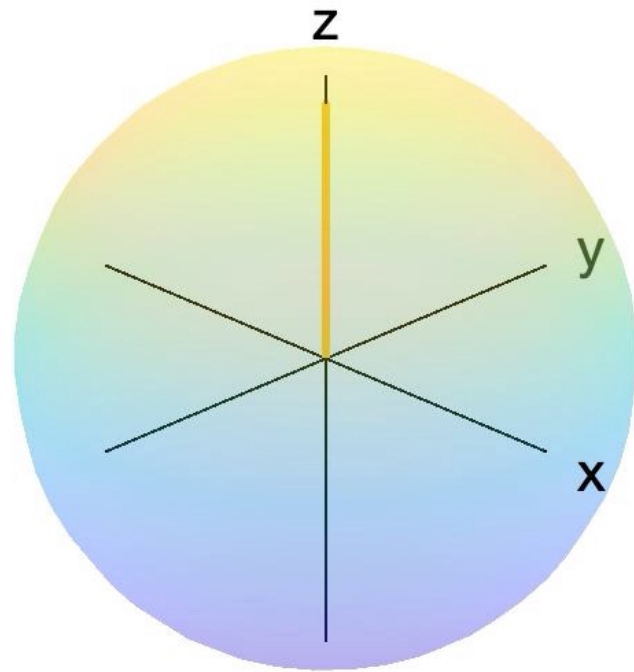
Apply RF pulse to tip magnetization from the z-axis into x-y plane  
Longitudinal Magnetization  $\rightarrow$  Transverse Magnetization



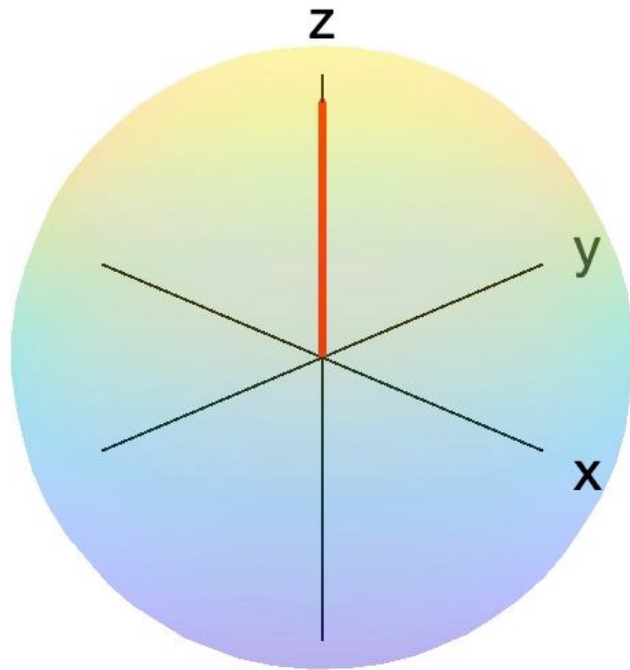
# Spin Lattice Relaxation: $T_1$



# Spin Lattice Relaxation: $T_1$

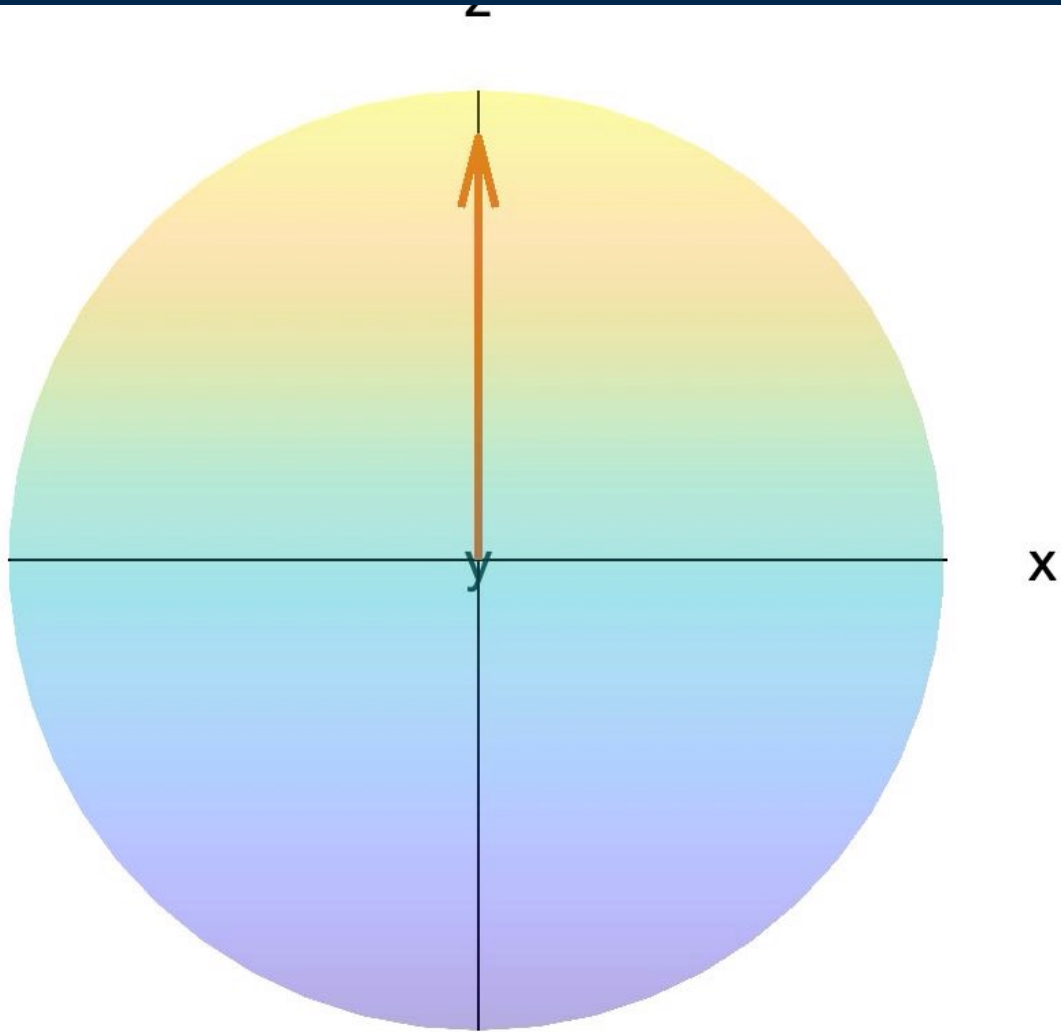


# Different Tissues Have Different $T_1$ Values



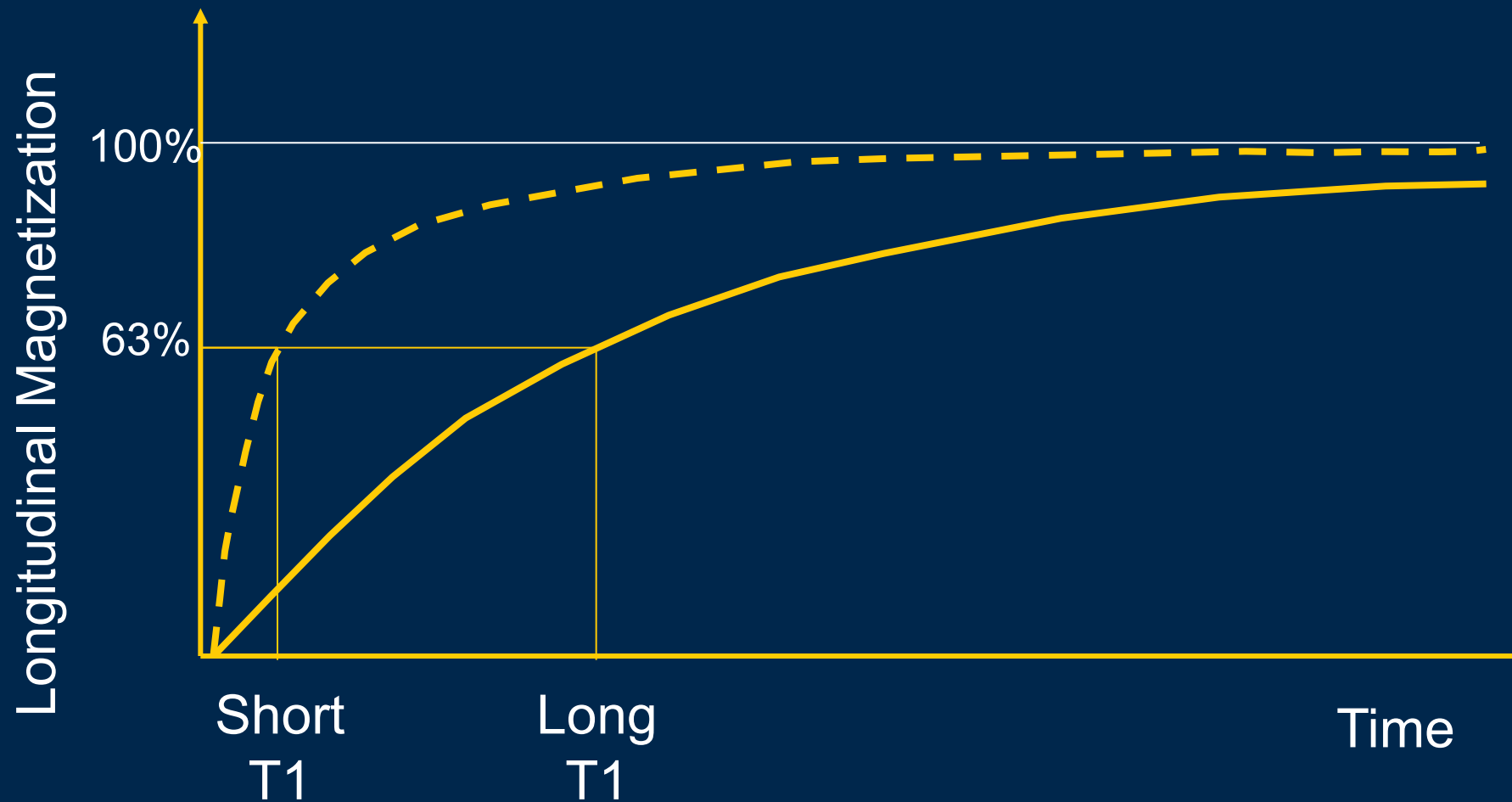
- Red  $\rightarrow$  Short  $T_1$
- Blue  $\rightarrow$  Long  $T_1$

# Different Tissues Have Different $T_1$ Values



- Red  $\rightarrow$  Short  $T_1$
- Blue  $\rightarrow$  Long  $T_1$

# Plot of Magnetization on z-axis after 90° Pulse



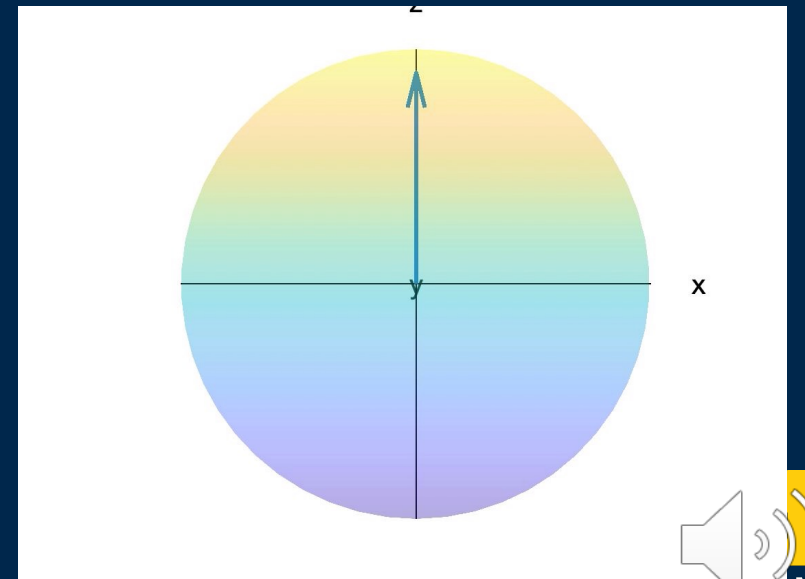
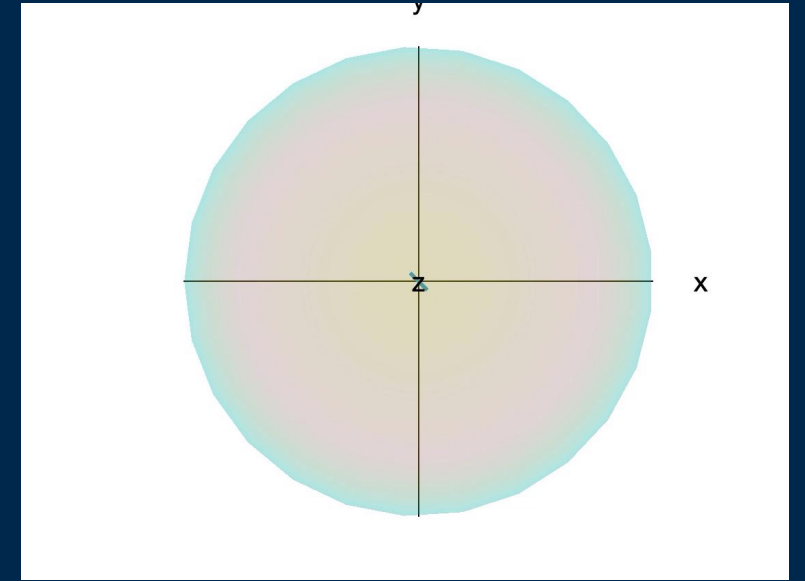
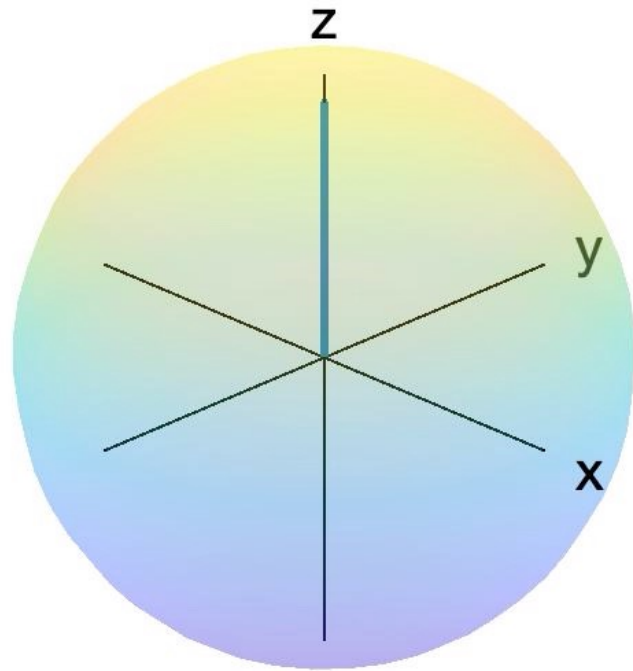
# Info about T1 times

- Not easily explained in terms of tissue content (molecular tumbling rates)
- Water content
- Measured in seconds or ms
- Different at different main field strengths
- Pure water → Long T1
- Fat → Shorter T1

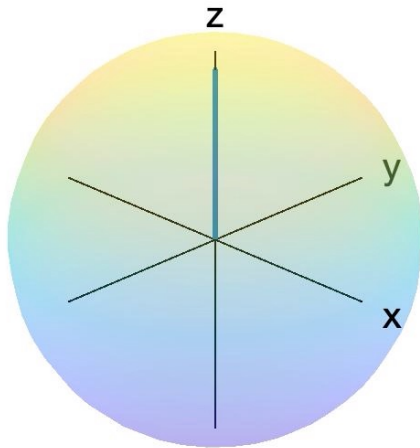
Tissue	T1 (msec)
Water/CSF	4000
Gray matter	900
Muscle	900
Liver	500
Fat	250
Tendon	400
Proteins	250
Ice	5000



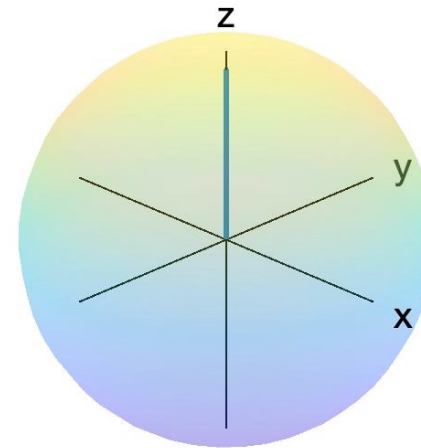
# Precession with T1 relaxation



# Rotating Reference Frame



Lab Reference Frame



Rotating Reference Frame

# T1 Relaxation Summary

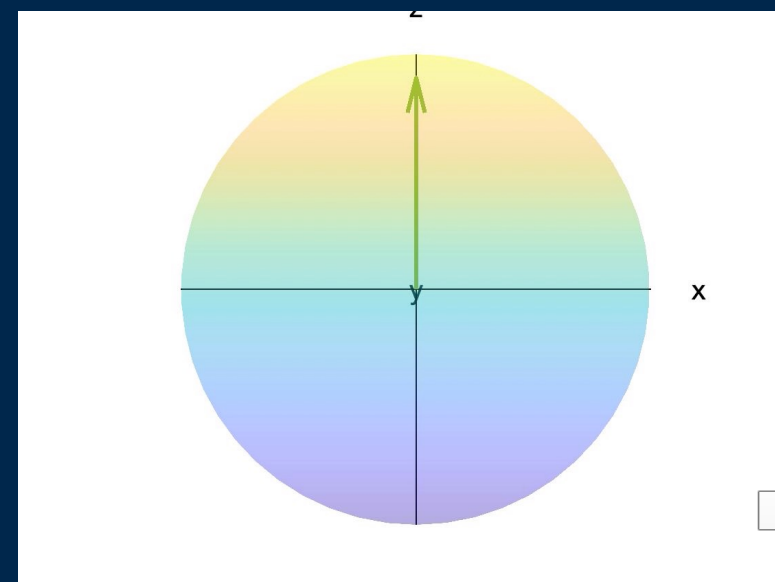
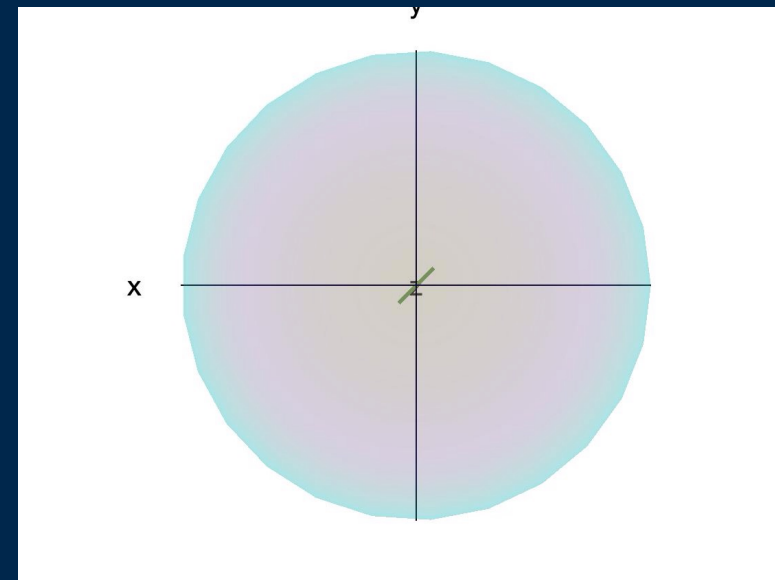
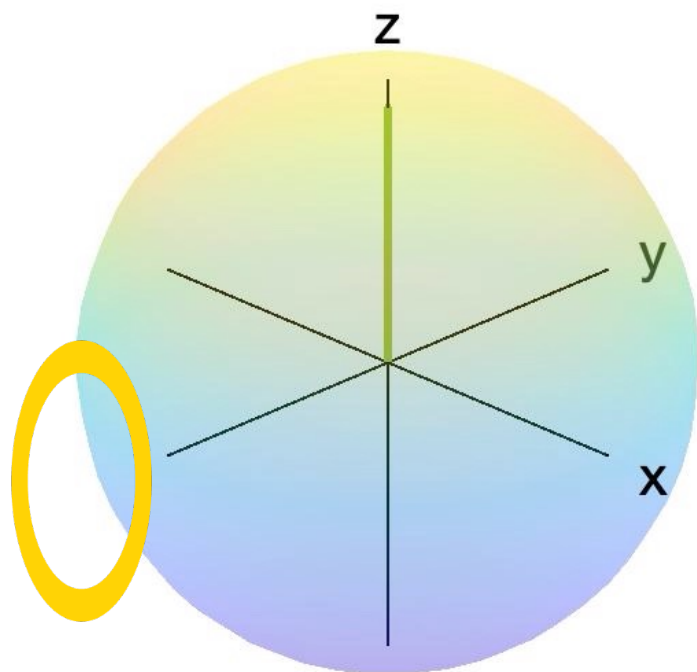
- T1 Relaxation (Spin-Lattice Relaxation)
  - Exponential recovery of Transverse to Longitudinal Magnetization
- Different tissues have different T1 relaxation rates
- ~ 250 ms – 5 seconds
- Main contrast mechanism in clinical imaging
- Pure water has a long T1

# MRI Physics:

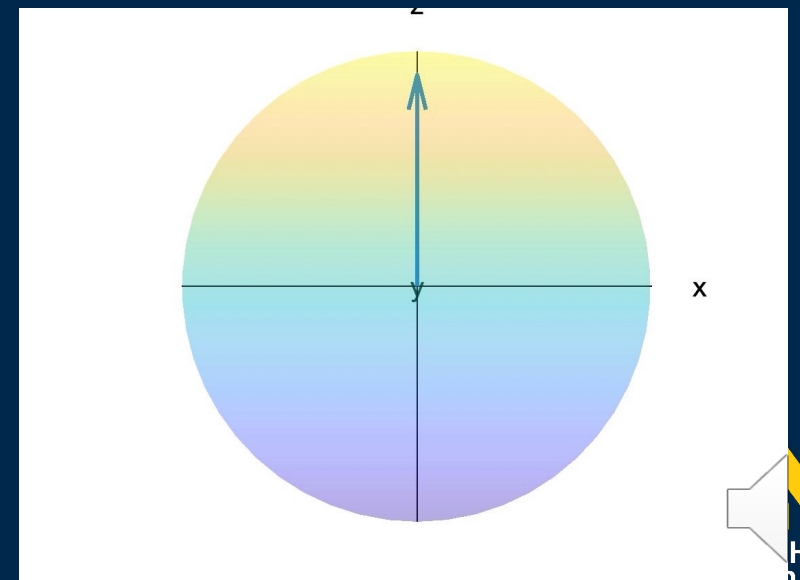
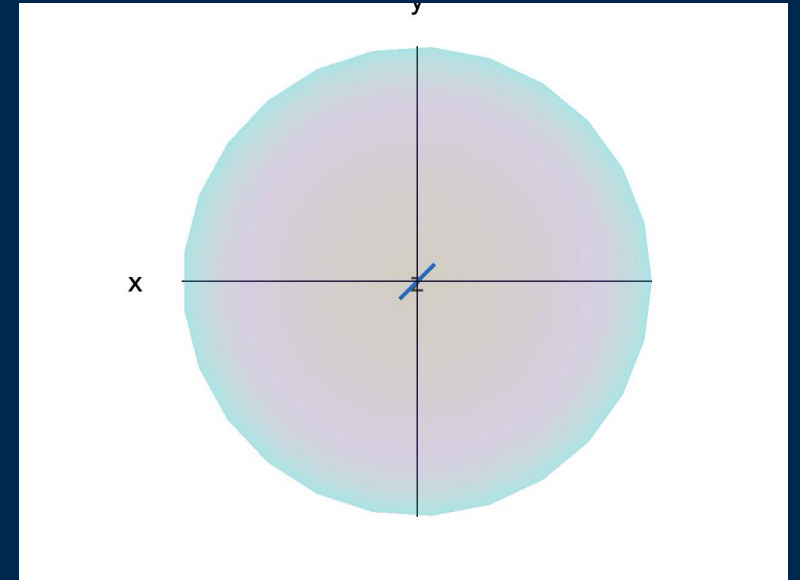
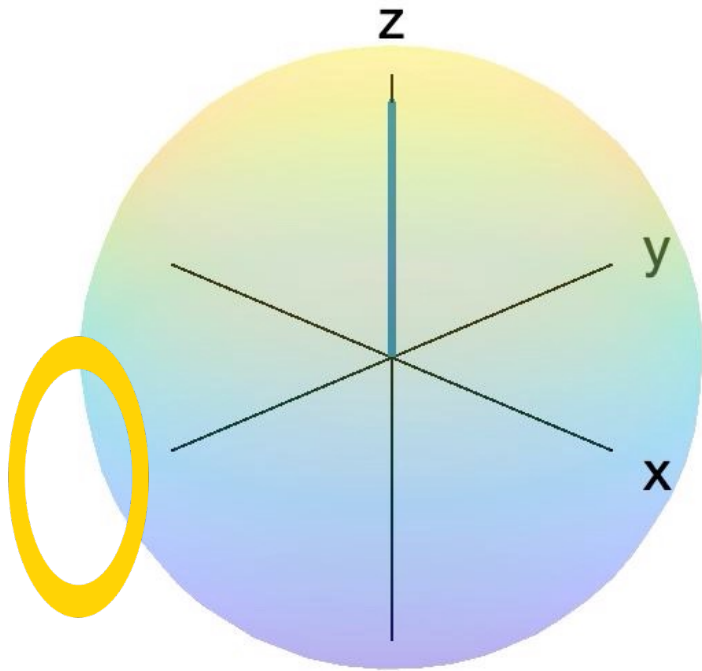
# T2 Relaxation

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# Spin-Spin Relaxation: $T_2$ (rotating reference frame)



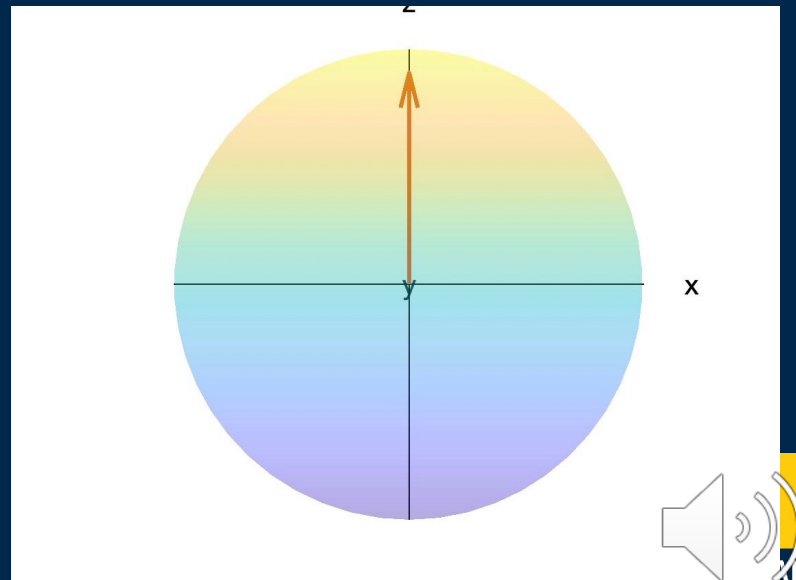
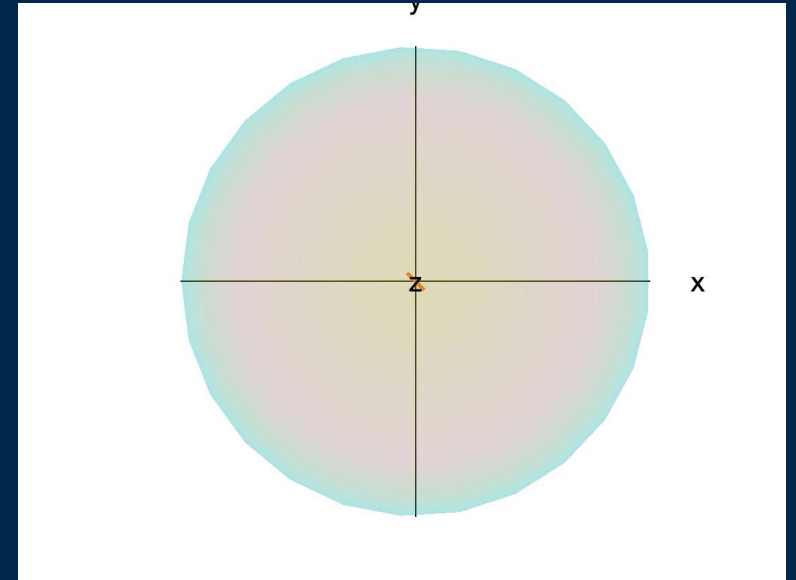
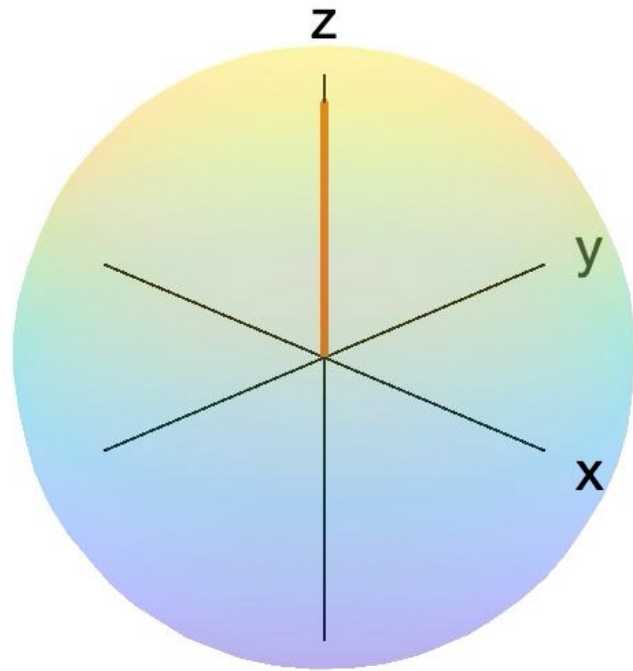
# We see vector sum of magnetization as signal



# Spin-Spin Relaxation: $T_2$

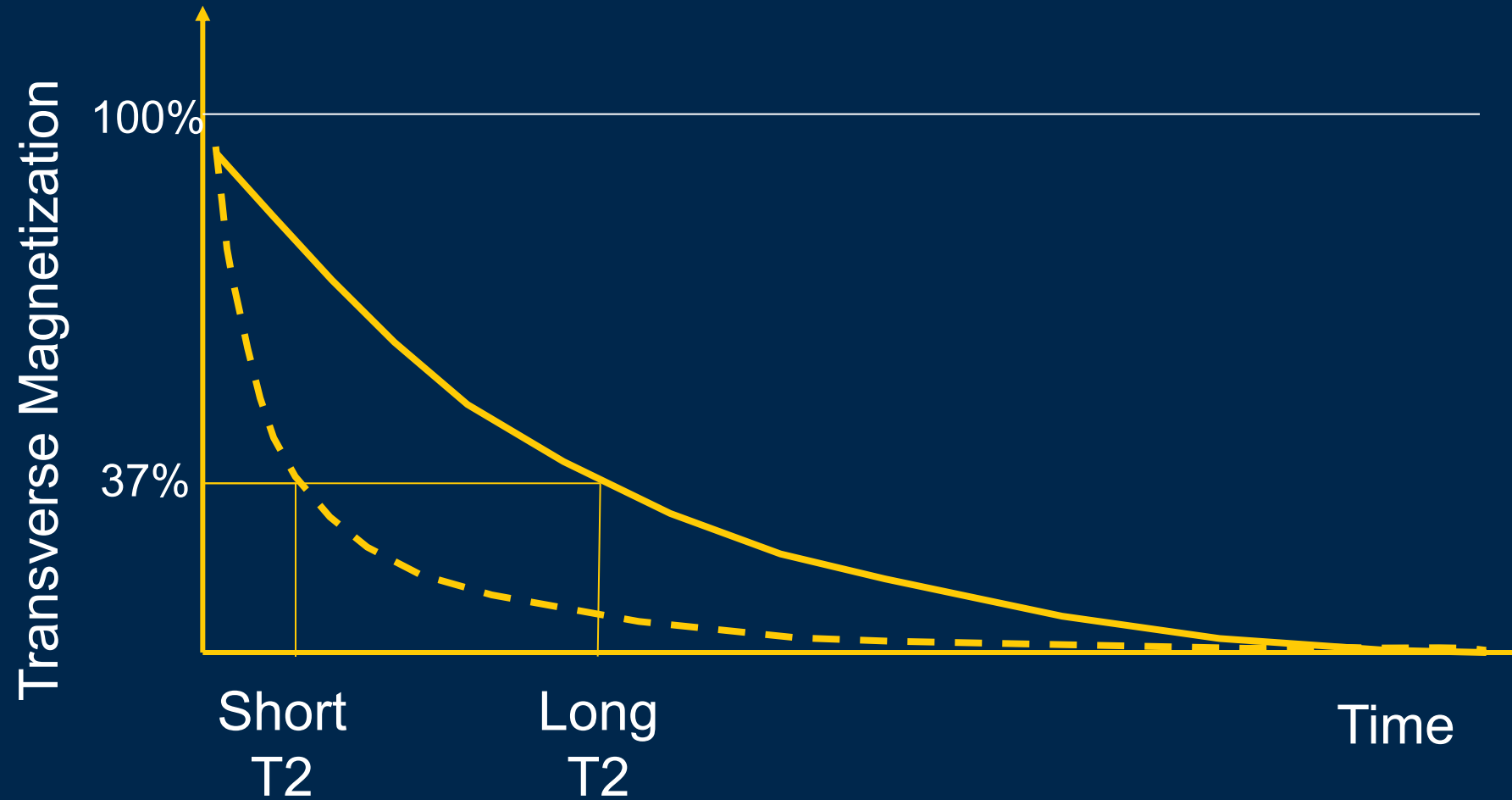
- Magnetization precesses according to Larmor frequency
- Precession freq of individual spins can be slightly altered due to small local magnetic field fluctuations
  - Spins fan out
  - "Dephasing"
- When measured together, this dephasing leads to signal loss
- Occurs at the same time (and faster than)  $T_1$  relaxation

# Different tissues have different $T_2$ values






# Plot of Magnetization on $xy$ -axis after $90^\circ$ Pulse



# Facts about $T_2$ Relaxation

- Not easily explained in terms of tissue content  
Much shorter in “solids”
- Measured in seconds or ms
- Different at different main field strengths
- Always shorter than  $T_1$
- Pure water  $\rightarrow$  Long  $T_2$

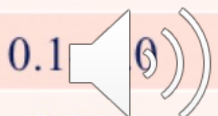
Tissue	$T_1$ (msec)	$T_2$ (msec)
Water/CSF	4000	2000
Gray matter	900	90
Muscle	900	50
Liver	500	40
Fat	250	70
Tendon	400	5
Proteins	250	0.1
Ice	5000	0.001



# More Facts about T<sub>2</sub> Relaxation

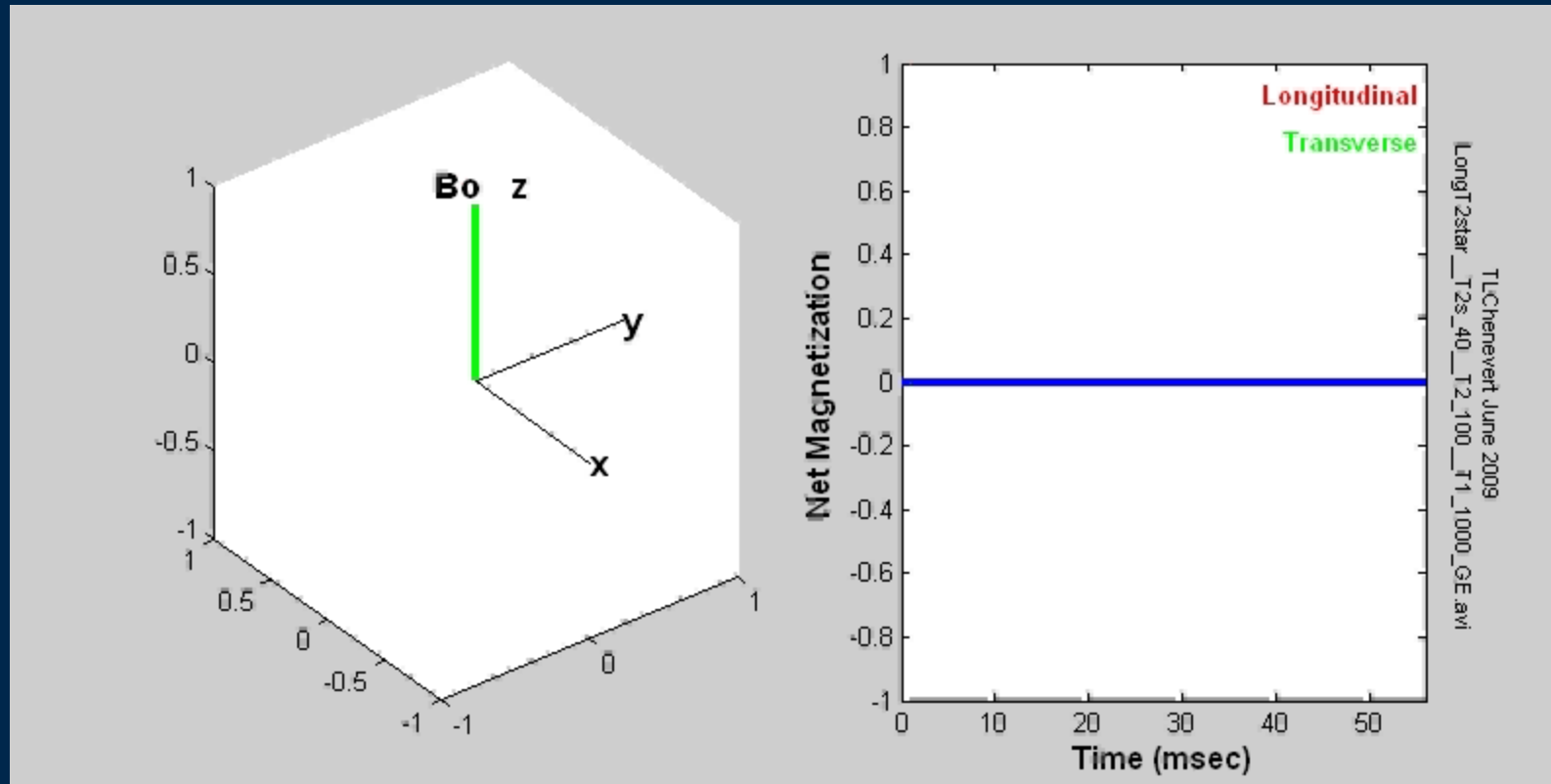
- T2 relaxation is a result of disorder in the system, not loss of magnetization  
→ Cannot be recovered
- T2' is a result of inhomogeneities in the magnetic field  
*metal clips/objects nearby, level of iron-content in tissue, differences in “magnetic susceptibility” (eg. bone vs air vs tissue)*  
→ Can in some cases be recovered
- T2 vs. T2\* contrast  
 $1/T2^* = 1/T2 + 1/T2'$   
T2\* always shorter than T2

Tissue	T1 (msec)	T2 (msec)
Water/CSF	4000	2000
Gray matter	900	90
Muscle	900	50
Liver	500	40
Fat	250	70
Tendon	400	5
Proteins	250	0.1
Ice	5000	0.001



# T2\* Relaxation: decay of transverse magnetization following an RF-pulse (aka free induction decay 'FID')

An example of "Long" T2\*~20-40ms



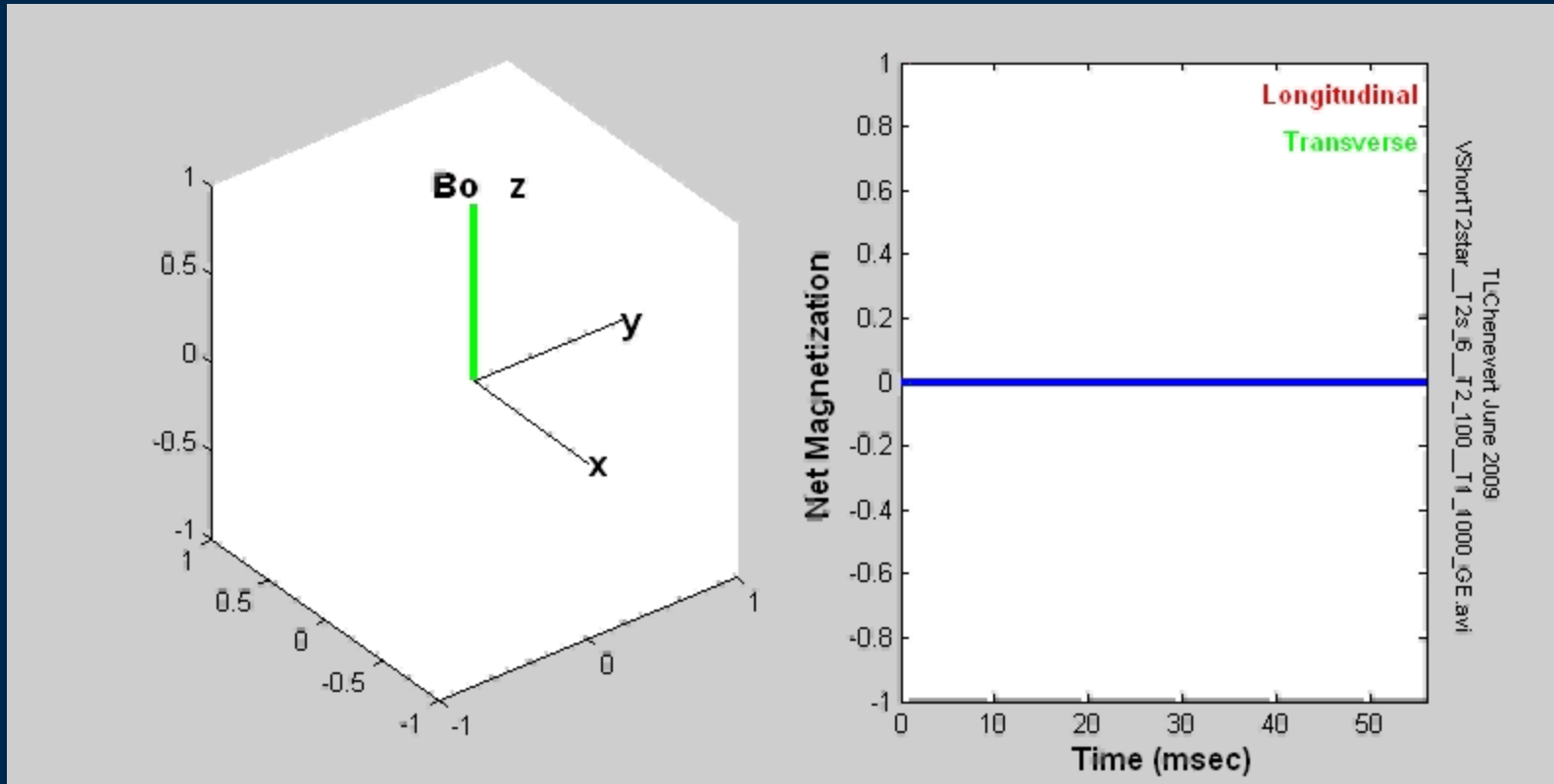
“Isochromats”  
(sub-voxel group of spins in  
equivalent local field)

Net Longitudinal Magnetization  
Net Transverse Magnetization (signal)

LongT2star\_T2s\_40\_T2\_100\_T1\_1000\_GE.avi

# T2\* Relaxation

An example of "Short" T2\*~1-10ms



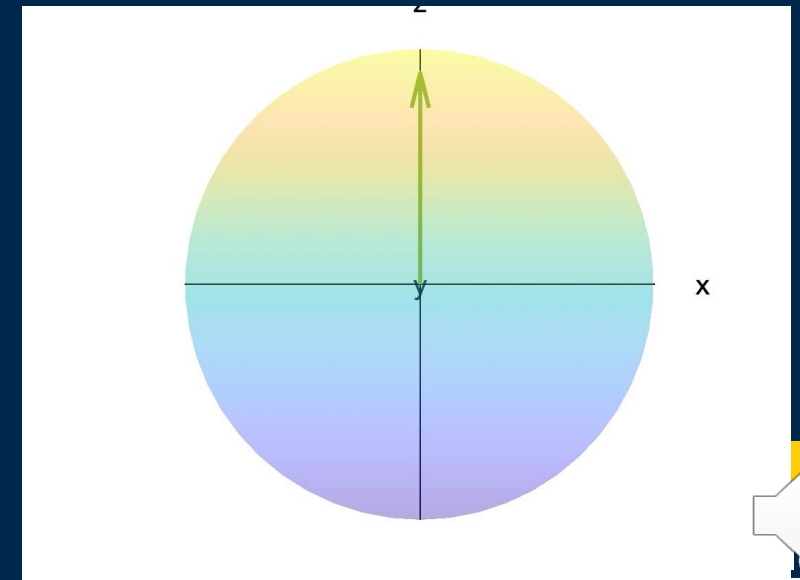
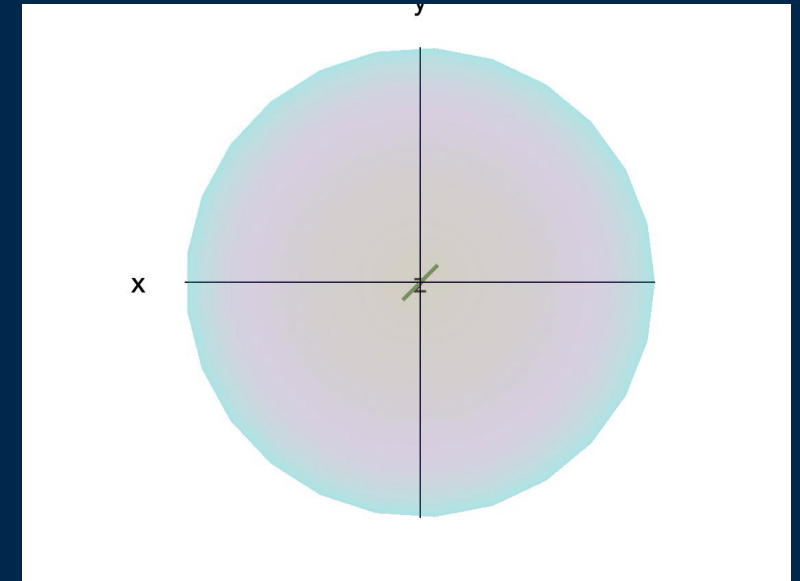
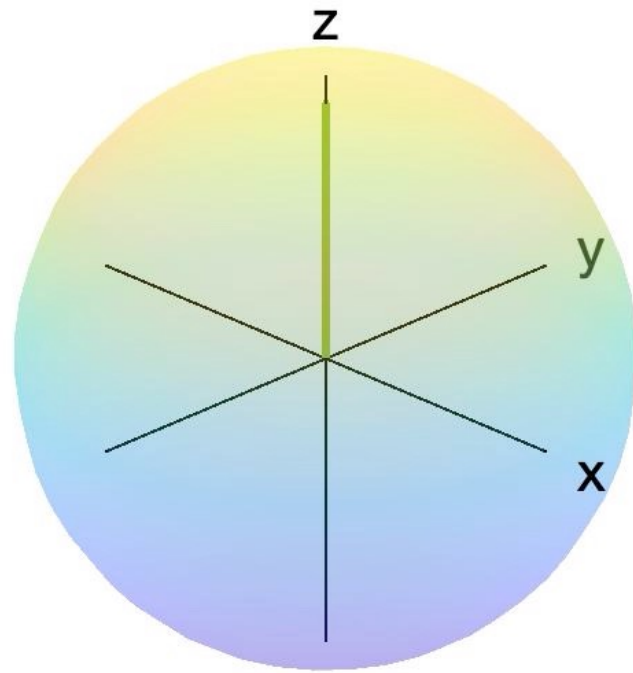
Isochromats

Net Longitudinal Magnetization  
Net Transverse Magnetization (signal)

# Recap: Magnetization

- Aligns along z-axis in direction of  $B_0$  field
- Can be tipped into x-y plane using an RF pulse
- Only transverse magnetization gives rise to signal
- Once in x-y plane, will precess at Larmor frequency (different for fat/ $H_2O$ )
- Slowly recovers back to the z-axis according to T1 value  
→ Loss of transverse magnetization, gain in longitudinal magnetization
- Dephases in x-y plane according to T2/T2\* value  
→ Loss of transverse magnetization

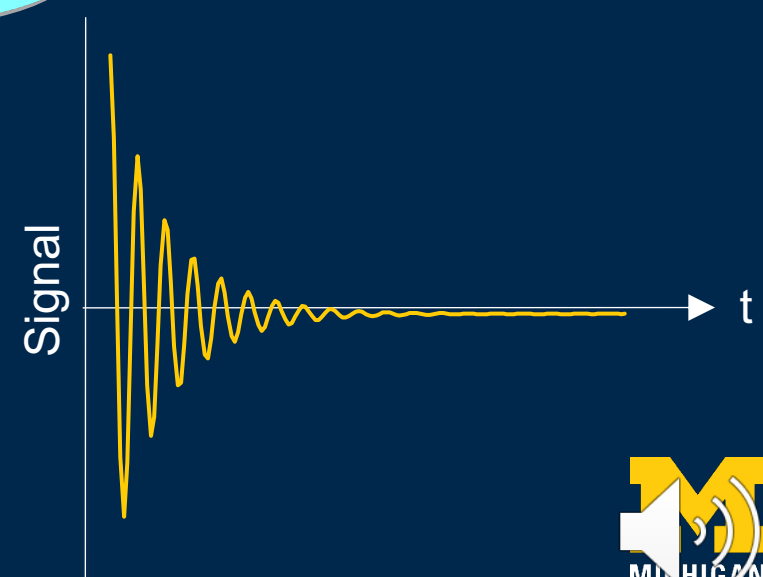
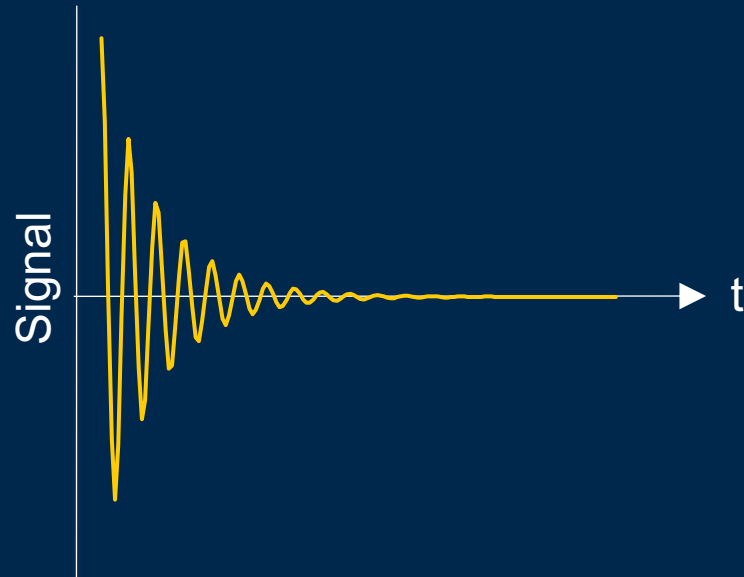
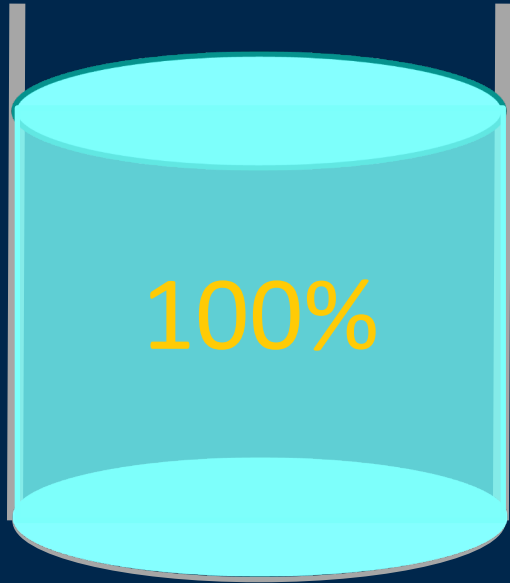
# All Effects Together (Precession, T1 and T2 Relaxation)



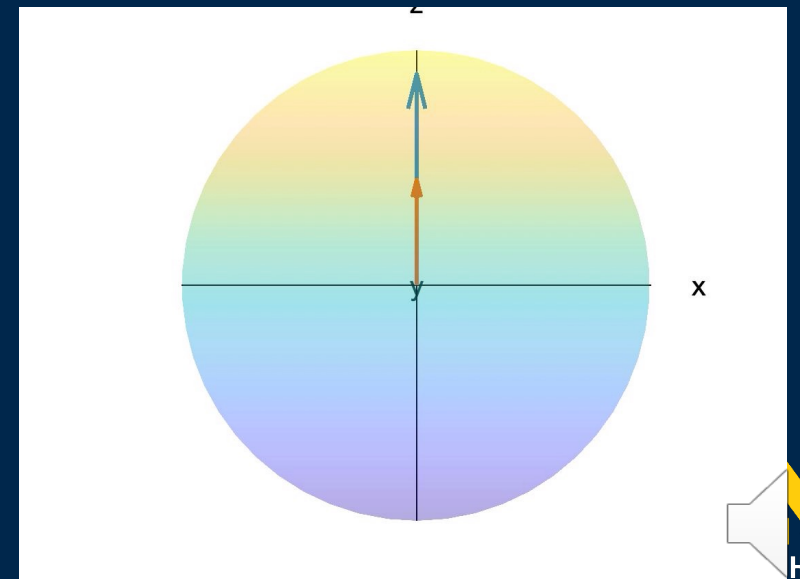
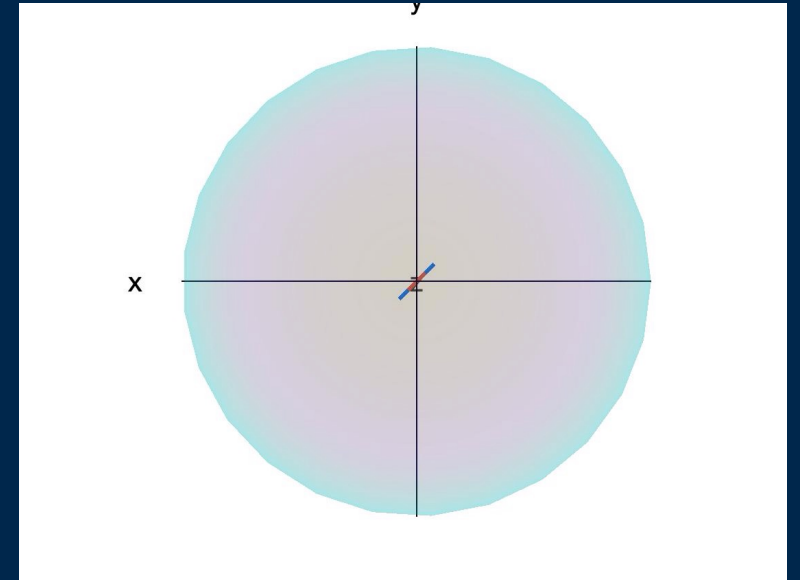
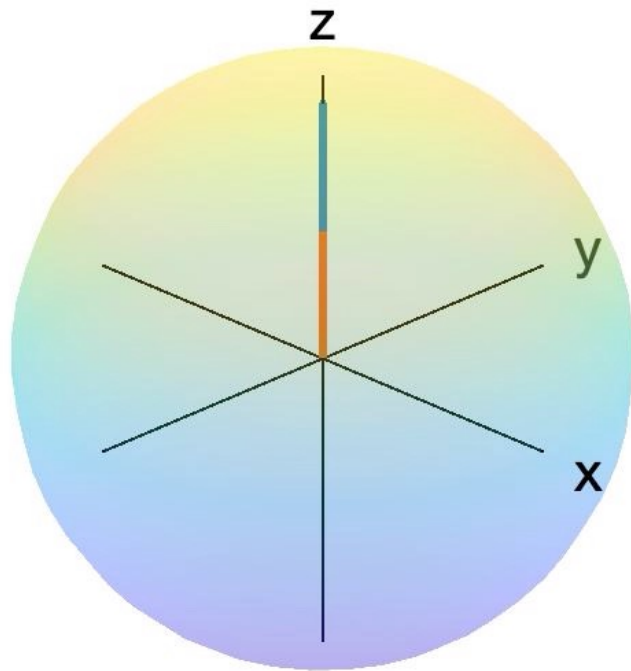
# Proton Density



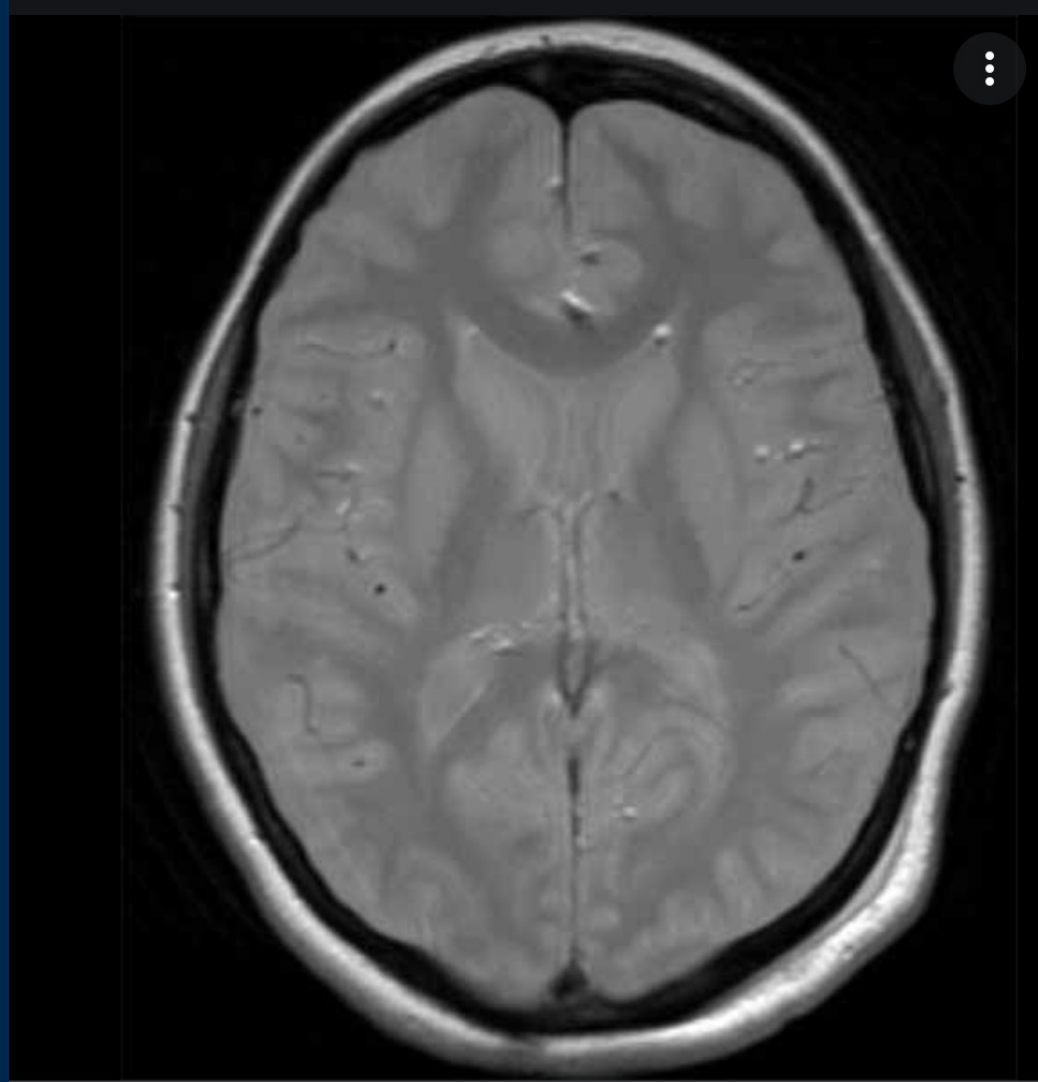
# The more protons, the more signal



# Differences in Proton Density give rise to contrast



# Differences in Proton Density give rise to contrast



But it is usually boring as most soft tissues have similar water content

# Summary of Proton Density ( $\rho$ )

- In addition to T1 and T2, MR images all contain “proton density” contrast
- Called Proton Density,  $M_0$ ,  $\rho$  ... all the same
- MRI signal is directly proportional to “number of protons” in a voxel
- Can also be used as a contrast mechanism (but usually fairly boring)